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Lentigo maligna (LM) is an *in situ* form of melanoma which can progress into invasive lentigo maligna melanoma (LMM). Variations in the pigmentation and thus visibility of the tumour make assessment of lesion borders challenging. We tested hyperspectral imaging system (HIS) in *in vivo* preoperative delineation of LM and LMM margins. We compared lesion margins delineated by HIS with those estimated clinically, and confirmed histologically. A total of 14 LMs and 5 LMMs in 19 patients were included. HIS analysis matched the histopathological analysis in 18/19 (94.7%) cases while in 1/19 (5.3%) cases HIS showed lesion extension not confirmed by histopathology (false positives). Compared to clinical examination, HIS defined lesion borders more accurately in 10/19 (52.6%) of cases (wider, \(n=7\) or smaller, \(n=3\)) while in 8/19 (42.1%) cases lesion borders were the same as delineated clinically as confirmed histologically. Thus, HIS is useful for the detection of subclinical LM/LMM borders. Key words: lentigo maligna; lentigo maligna melanoma; tumour margin assessment; hyperspectral imaging.

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Delineating Margins of Lentigo Maligna Using a Hyperspectral Imaging System

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Fig. 1. Hyperspectral imaging process and data analysis. Hyperspectral image (cube) consists of overlapping images, of which each is taken at different wavelength. Each pixel in the hyperspectral image has its own spectral signature. Mathematical algorithms (VCA, FVA) are used to separate the spectra (endmembers) of benign and malignant tissue. The abundance images represent the areas of lesional and healthy skin.
Different biological tissues can be identified from their unique spectral signatures reflecting their biochemical characteristics (6–8). This pilot study aimed to test the feasibility of the HIS in delineation of the margins of LM and LMM preoperatively in order to avoid the need for re-excisions.

MATERIALS AND METHODS

Patients

The study protocol followed the Declaration of Helsinki and was approved by the local ethics committee. All volunteering patients provided their written informed consent. The patients were recruited from those remitted to the Department of Dermatology for their suspected LMs.

Nineteen patients, 7 women and 12 men, with clinically suspect LM or LMM located on their faces or scalps were included in the study. The patients' mean age was 77.9 (range 67–97 years). Three patients displayed skin photo-type I, 8 photo-type II, and 8 photo-type III (9). Nine patients out of 19 had earlier been treated for a non-melanoma skin cancer or premalignant skin lesions (basal cell carcinoma \( n = 2 \), actinic keratosis \( n = 2 \) or both \( n = 5 \)). None of the patients had earlier been treated for melanoma.

Clinical assessment of the lesion borders using digital imaging and Wood’s light examination

Prior to the imaging processes lesions were evaluated using dermatoscopy (Dermlite® DL3). Clinical assessment of the lesion borders was carried out using Wood’s light examination (Burton®) and digital photography (Canon Ixus 130, 14.1 megapixel).

Hyperspectral imaging system and image analysis

All 19 lesions were imaged prior to surgical removal using HIS. The used handheld HIS was developed for the study at the VTT Technical Research Centre of Finland and University of Jyväskylä, Finland. This prototype imaging system consisted of a hyperspectral imager (500–850 nm) (10, 11), external light source of visible and infrared light, fibre optic ring light and a holder for the imager and the ring light. The field of view was 12 cm². HIS acquired the diffuse reflectance of the detected skin areas rapidly in a few seconds. The acquired hyperspectral data cube was analysed using an assumption of the linear mixture model (vertex component analysis, VCA and filter vector algorithm FVA) (12–14) to achieve pure spectra (endmembers) of LM/LMM and healthy skin (Fig. S1¹) and to produce abundance maps for delineation of the lesion borders (Fig. 2, Fig. S2¹). The hyperspectral imager and the analysing process are shown in Fig. 1, and detailed in Appendix S1¹.

Histopathological sampling

The lesions of 5/19 patients were biopsied before recruiting to the study and excised immediately after the imaging processes. The edges of the specimens were marked with orienting sutures, and inked for orientation. To help mapping the findings for 14/19 patients, we took targeted 3 mm punch biopsies (2–4 per patient) from the middle and from lesions borders, defined using the HIS, and afterwards the lesions were completely excised with wide excision margins. The biopsy sites and excision margins were marked and photographed. An experienced dermatopathologist (LJ) examined the samples without any background information.

RESULTS

The comparative analyses included a total of 14 LMs and 5 LMMs located on the face and scalp (nose \( n = 1 \), ear \( n = 4 \), eyelid \( n = 2 \), forehead \( n = 2 \) and on the cheek area \( n = 10 \)) of 19 patients. The invasion depth (Breslow thickness) of the LMMs varied between 0.5 and 1.25 mm. The mean lesion area was 2.4 cm² (range 1.6–7.6 cm²).

In the delineation of LM or LMM margins, HIS analysis matched the histopathological analysis in 18/19 (94.7%) patients.

¹http://www.medicaljournals.se/acta/content/?doi=10.2340/00015555-2010
cases while in 1/19 (5.3%) cases HIS showed lesion extension not confirmed by histopathology (false positives). In 10/19 (52.6%) of the cases lesion margins were delineated more accurately (wider, \( n = 7 \) or smaller, \( n = 3 \)) by HIS than by clinical examination with Wood’s light, as confirmed by histopathological analysis (Fig 2, Fig S2'). In 8/19 (42.1%) cases the lesion margins were equally delineated by HIS and clinical examination, as confirmed by histopathology. No false negatives were detected when comparing HIS detection with histopathology.

In the false positive case an actinic keratosis and benign lentigo was present histologically on the LM borders which complicated the interpretation of the HIS image.

The lesions were operated in accordance with current standards by removing LMs with 5 mm clinical margins and LMMs with 10 mm margins if anatomically possible (15). As this was a pilot study, the margins given by HIS were not used in the excisions. After receiving the results from the histopathological analyses, 3/14 of the LM lesions and 2/5 LMM lesions needed re-excision because of the subclinical extension of the lesion borders. If the excision borders had been selected on the basis of the HIS analysis, 5 re-excisions could have been avoided (Table I).

### DISCUSSION

This study indicates that the HIS is capable of detecting the subclinical borders of LM and LMM. Importantly, in over 50% of the cases, the lesion margins were assessed more accurately by using the HIS than with the clinical methods. The advantages of HIS include a handheld imager with a large field of view (12 cm²) and a quick imaging process. All studied skin areas including the nose and ears were suitable for imaging with the HIS and fitted the field of view.

The lesions were removed with margins determined after delineating the tumour visually using Wood’s light. Three LM patients and 2 LMM patients needed re-excision because of the histologically verified subclinical extension of the lesions. Interestingly, if the patients had initially been operated on using margins given by HIS, the re-excisions could have been avoided. HIS also seems to be inversely useful, since clinical assessments delineated 3 LM lesions incorrectly larger than depicted using HIS and confirmed by histopathology.

Discrimination of LM from sun-damaged skin at the periphery of lesions may also be challenging histologically (3). The cytological atypia in LM may vary and be subtle. The diffuse melanocytic overgrowth of sun-damaged skin and the presence of benign melanocytes along the hair follicles make it challenging to assess the peripheral margins of LM. Immunohistochemistry, for e.g. MART-1, is sometimes used to identify LM. However, also normal, chronically sun-exposed skin has a high number of MART-1 positive melanocytes (16, 17). In one case in our study, benign lentigines and subclinical AK surrounding the LM made it difficult to correctly interpret the HIS image and led to a false positive interpretation. These lesions might have complicated the histopathological analysis as well.

Wood’s light turned out to be of only marginal help in assessing the margins of LMs. Especially in cases where also benign lentigines were present, the delineation of LM with Wood’s light was complicated. Since both melanin and haemoglobin strongly absorb visible and UV light (4), a future developmental aspect could be to integrate a UV light source to HIS to improve visualisation of the pigmentation.

There are several commercially available devices for skin cancer detection and a magnitude of research in the field (18, 19). As far as we know there are no commercial applications of a HIS. Previously, a few techniques have been used to assess surgical margins including: dermatoscopy, confocal microscopy and optical coherence tomography.

**Dermatoscopy** (epiluminescence microscopy) helps in defining the LM borders, but requires an experienced dermatoscopist (20). LM on the face do not show the classical dermoscopic features found on the other parts of the skin, which makes their observation more challenging (21). In this study dermatoscopy was used as a diagnostic aid, but not for the delineation of the lesions.

**Confocal microscopy** has shown potential in evaluating pigmented skin lesions and their margins (22). The device detects to depths of 300 μm, i.e. to the papillary

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**Table I. Lesion characteristics in hyperspectral images (HIS) compared with clinical evaluation**

<table>
<thead>
<tr>
<th>Patient</th>
<th>Breslow thickness (mm)</th>
<th>HIS provided no additional information</th>
<th>False positive</th>
<th>Re-excision avoidable</th>
</tr>
</thead>
<tbody>
<tr>
<td>1</td>
<td>In situ</td>
<td>Smaller</td>
<td>–</td>
<td>–</td>
</tr>
<tr>
<td>2</td>
<td>In situ</td>
<td>Smaller</td>
<td>–</td>
<td>–</td>
</tr>
<tr>
<td>3</td>
<td>In situ</td>
<td>–</td>
<td>–</td>
<td>–</td>
</tr>
<tr>
<td>4</td>
<td>In situ</td>
<td>–</td>
<td>–</td>
<td>–</td>
</tr>
<tr>
<td>5</td>
<td>In situ</td>
<td>–</td>
<td>–</td>
<td>–</td>
</tr>
<tr>
<td>6</td>
<td>In situ</td>
<td>–</td>
<td>–</td>
<td>–</td>
</tr>
<tr>
<td>7</td>
<td>In situ</td>
<td>–</td>
<td>–</td>
<td>–</td>
</tr>
<tr>
<td>8</td>
<td>In situ</td>
<td>–</td>
<td>–</td>
<td>–</td>
</tr>
<tr>
<td>9</td>
<td>In situ</td>
<td>Smaller</td>
<td>–</td>
<td>–</td>
</tr>
<tr>
<td>10</td>
<td>In situ</td>
<td>Smaller</td>
<td>–</td>
<td>–</td>
</tr>
<tr>
<td>11</td>
<td>In situ</td>
<td>–</td>
<td>–</td>
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</tr>
<tr>
<td>12</td>
<td>In situ</td>
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<tr>
<td>13</td>
<td>In situ</td>
<td>–</td>
<td>–</td>
<td>–</td>
</tr>
<tr>
<td>14</td>
<td>In situ</td>
<td>Smaller</td>
<td>–</td>
<td>–</td>
</tr>
<tr>
<td>15</td>
<td>In situ</td>
<td>Smaller</td>
<td>–</td>
<td>–</td>
</tr>
<tr>
<td>16</td>
<td>In situ</td>
<td>–</td>
<td>–</td>
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</tr>
<tr>
<td>17</td>
<td>In situ</td>
<td>–</td>
<td>–</td>
<td>–</td>
</tr>
<tr>
<td>18</td>
<td>In situ</td>
<td>–</td>
<td>–</td>
<td>–</td>
</tr>
<tr>
<td>19</td>
<td>In situ</td>
<td>–</td>
<td>–</td>
<td>–</td>
</tr>
</tbody>
</table>

\(^{1}\)HIS shows lesion margins more accurately compared to clinical evaluation as confirmed histologically. \(^{2}\)Lesion borders similarly detected clinically, by HIS and histology. \(^{3}\)HIS shows lesion wider than histologically confirmed. \(^{4}\)Only minor subclinical extension, no need for re-excision.
dermis. The limitation in confocal microscopy is a small field of view (FOV 8 × 8 mm mosaic composite images) leading to several slow imaging sessions for each lesion. The method lacks any objective analysis and the assessment of one FOV area requires at least 5 min for an expert which makes the method slow compared to HIS (23, 24).

**Optical coherence tomography** (OCT), has shown potential in delineating the borders of non-melanocytic skin malignancies (25). As far as we know there are no studies of the delineation of pigmented lesions using OCT. The device provides high-resolution cross-sectional images at greater depths (1.5–2 mm) than confocal microscopy. The FOV is small (6 × 6 mm), thus making the imaging process slower than in HIS. The analysis remains subjective.

We have earlier shown that the HIS is useful in the detection of skin field cancerisation (5). In the present study HIS showed its potential in the detection of the subclinical borders of LM and LMM. By detecting ac-sudy HIS showed its potential in the detection of the skin field cancerisation (5). In the present remains subjective.

REFERENCES

The authors declare no conflicts of interest.

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The authors declare no conflicts of interest.

REFERENCES